



## King's Research Portal

DOI:

[10.1016/j.jvs.2019.02.063](https://doi.org/10.1016/j.jvs.2019.02.063)

*Document Version*

Peer reviewed version

[Link to publication record in King's Research Portal](#)

*Citation for published version (APA):*

Tossas-Betancourt, C., van Bakel, T. M. J., Arthurs, C. J., Coleman, D. M., Eliason, J. L., Figueroa, C. A., & Stanley, J. C. (2020). Computational analysis of renal artery flow characteristics by modeling aortoplasty and aortic bypass interventions for abdominal aortic coarctation. *Journal of Vascular Surgery*, 71(2), 505-516.e4. <https://doi.org/10.1016/j.jvs.2019.02.063>

### **Citing this paper**

Please note that where the full-text provided on King's Research Portal is the Author Accepted Manuscript or Post-Print version this may differ from the final Published version. If citing, it is advised that you check and use the publisher's definitive version for pagination, volume/issue, and date of publication details. And where the final published version is provided on the Research Portal, if citing you are again advised to check the publisher's website for any subsequent corrections.

### **General rights**

Copyright and moral rights for the publications made accessible in the Research Portal are retained by the authors and/or other copyright owners and it is a condition of accessing publications that users recognize and abide by the legal requirements associated with these rights.

- Users may download and print one copy of any publication from the Research Portal for the purpose of private study or research.
- You may not further distribute the material or use it for any profit-making activity or commercial gain
- You may freely distribute the URL identifying the publication in the Research Portal

### **Take down policy**

If you believe that this document breaches copyright please contact [librarypure@kcl.ac.uk](mailto:librarypure@kcl.ac.uk) providing details, and we will remove access to the work immediately and investigate your claim.

1 **COMPUTATIONAL ANALYSIS OF RENAL ARTERY FLOW CHARACTERISTICS**  
2 **BY MODELING AORTOPLASTY AND AORTIC BYPASS INTERVENTIONS FOR**  
3 **ABDOMINAL AORTIC COARCTATION**  
4

5  
6  
7 Christopher Tossas-Betancourt<sup>1\*</sup>, Theodorus M.J. van Bakel<sup>2\*</sup> MD, Christopher J. Arthurs<sup>3</sup> DPhil,  
8 Dawn M. Coleman<sup>2</sup> MD, Jonathan L. Eliason<sup>2</sup> MD, C. Alberto Figueroa<sup>1,2</sup> PhD, James C. Stanley<sup>2</sup>  
9 MD  
10

11  
12  
13  
14  
15 \* Contributed equally.  
16

17 Departments of <sup>1</sup>Biomedical Engineering and <sup>2</sup>Surgery, University of Michigan, Ann Arbor,  
18 Michigan; <sup>3</sup>Division of Imaging Sciences and Biomedical Engineering, King's College London,  
19 London, UK  
20

21 Presented at the 42<sup>nd</sup> Annual Meeting of the Midwestern Vascular Surgical Society, St. Louis,  
22 Missouri, September 13, 2018.  
23

24 Funding statement: This work was supported by the European Research Council under the  
25 European Union's Seventh Framework Programme (FP/2007-2013) [ERC Grant Agreement No.  
26 307532]; by grants from the NIH (R01 HL105297, U01 HL135842) the Edward B. Diethrich  
27 Professorship; the Bob and Ann Aikens Aortic Grants Program; and the Frankel Cardiovascular  
28 Center. Computing resources were provided by the National Science Foundation [grant 1531752]  
29 Acquisition of Conflux, A Novel Platform for Data-Driven Computational Physics (Tech.  
30 Monitor: Ed Walker).  
31

32 Disclosures: All authors declare no conflicts of interest related to the contents of the manuscript.  
33

34 Corresponding author: C. Alberto Figueroa, 2800 Plymouth Road Building 20-210W, Ann Arbor,  
35 Michigan, 48105. E-mail: [figueroc@med.umich.edu](mailto:figueroc@med.umich.edu), Tel: +1.734.548.1660, Fax:  
36 +1.734.232.1234  
37  
38  
39

## 1 ARTICLE HIGHLIGHTS

2

3 **Type of Research: 1.** Single-center retrospective case  
4 study

5

6 **Key Findings:** Supra-renal abdominal aortic coarctation  
7 (SAAC) was associated with high frequency disturbances  
8 in the renal arteries that could trigger increased renin  
9 release in the kidneys, leading to secondary hypertension.  
10 In general, surgical repair reduced but not eliminated  
11 these disturbances.

12

13 **Take home Message:** High frequency disturbances in the  
14 renal arteries could explain the limited hypertension  
15 success rates of surgical repair for SAAC. Patient-  
16 specific computational modeling offers a valuable tool to  
17 analyze complex hemodynamics in vascular disease and  
18 test the hemodynamic performance of different surgical  
19 interventions.

20

## 21 Table of Contents Summary

22

23 This retrospective case study used analyzed aortorenal  
24 hemodynamics in a patient with a SAAC and found that  
25 SAAC is associated with high frequency disturbances in  
26 the renal arteries that could trigger renin release, resulting  
27 in secondary hypertension. Surgical repair with TAB or  
28 PA reduces aortic pressures, but does not always  
29 eliminate the high frequency disturbances, explaining the  
30 limited hypertension success rates of these procedures.

31

32

33

34

35

36

37

38

## 1 **ABSTRACT**

2 **Objectives:** Suprarenal abdominal aortic coarctation (SAAC) alters flow and pressure patterns to  
3 the kidneys and is often associated with severe angiotensin-mediated hypertension, refractory to  
4 drug therapy. SAAC is most often treated by a thoracoabdominal bypass (TAB) or patch  
5 aortoplasty (PA). It is currently unclear what effect these interventions have on renal flow and  
6 pressure waveforms. This study, using retrospective data from a SAAC patient subject to a TAB,  
7 undertook computational modeling to analyze aortorenal blood flow preoperatively as well as  
8 postoperatively following a variety of TAB and PA interventions.

9 **Methods:** Patient-specific anatomical models were constructed from preoperative computed  
10 tomographic angiograms of a 9-year old child with an isolated SAAC. Fluid-structure interaction  
11 (FSI) simulations of hemodynamics were performed to analyze preoperative renal flow and  
12 pressure waveforms. A parametric study was then performed to examine the hemodynamic impact  
13 of different bypass diameters and patch oversizing.

14 **Results:** Preoperative FSI results documented diastolic-dominated renal perfusion with  
15 considerable high frequency disturbances in blood flow and pressure. The postoperative TAB right  
16 and left kidney volumes increased by 58% and 79%, respectively, reflecting the increased renal  
17 artery blood flows calculated by the FSI analysis. Postoperative increases in systolic flow  
18 accompanied decreases in high frequency disturbances, aortic pressure and collateral flow  
19 following all surgical interventions. In general, lesser degrees of high frequency disturbances  
20 followed PA interventions. High frequency disturbances were eliminated with the 0% PA, in  
21 contrast to the 30% and 50% PA oversizing and TAB interventions in which these flow  
22 disturbances remained.

1 **Conclusions:** Both TAB and PA dramatically improved renal artery flow and pressure waveforms,  
2 although disturbed renal waveforms remained in many of the surgical scenarios. Importantly, only  
3 the 0% PA oversizing scenario eliminated all high frequency disturbances, resulting in near normal  
4 aortorenal blood flow. The study also establishes the relevance of patient-specific computational  
5 modeling when planning interventions for the midaortic syndrome.

6

7

8

9

#### 10 **Clinical Relevance.**

11 We performed computational fluid dynamics (CFD) modeling to assess aortorenal blood flow in a  
12 child with a supra-renal abdominal aortic coarctation (SAAC) and test the performance of different  
13 surgical interventions. We discovered high-frequency disturbances in the renal arteries that could  
14 potentially triggering excessive renin release. Thoracoabdominal bypass and patch aortoplasty  
15 with oversizing did not remove these disturbances completely. This could explain why the  
16 hypertension cure rates of surgical repair of SAAC are suboptimal. Additionally, this study  
17 establishes the relevance of CFD modeling as a valuable tool to analyze complex hemodynamics  
18 and test the performance different surgical interventions.

19

## 1 INTRODUCTION

2           Suprarenal abdominal aortic coarctations (SAAC) are often associated with renal arterial  
3 stenoses and severe renin-mediated arterial hypertension.<sup>1</sup> In these circumstances, the increased  
4 blood pressure and development of collateral vessels circumventing the aortic and renal artery  
5 narrowings tend to increase mean renal blood flow toward normal. However, this response is  
6 inadequate and the abnormal release of renin persists. Whether the principal cause of the abnormal  
7 renin release is due to decreased renal artery pressure or abnormal renal artery flow waveforms is  
8 an unsettled issue.

9           The abnormal renin release and angiotensin generation coupled with secondary increases  
10 in aldosterone production make this form of hypertension refractory to most drug therapies.  
11 Lowering the systemic arterial pressure with drugs without treating the aortic and renal artery  
12 narrowings only results in further diminutions of intrarenal blood flow and continued excesses in  
13 renin production. Because of these medical failures, restoration of normal renal blood flow by  
14 open operative or endovascular interventions have evolved as the favored means of managing this  
15 disease.

16           The University of Michigan's history of treating occlusive lesions of the renal arteries and  
17 abdominal aorta in pediatric patients has extended for more than 4 decades.<sup>1-6</sup> Postoperative blood  
18 pressure control in this experience has been optimal when treating patients with isolated renal  
19 artery stenoses, in contrast to less salutary outcomes when the renal artery procedures have been  
20 accompanied by a thoracoabdominal bypass (TAB) or patch aortoplasty (PA) for a coexisting  
21 abdominal aortic coarctation. Even after successful anatomic aortic and renal artery  
22 reconstructions, postoperative hypertension has been noted to persist.<sup>1,7,8</sup>

1           It is hypothesized that the aortic reconstructive procedures may not normalize renal artery  
2 blood flow. A TAB from above a SAAC to below the renal arteries may cause turbulent and  
3 abnormal renal artery perfusion as retrograde aortic flow encounters antegrade flow in the region  
4 of the renal vasculature. In addition, performance of a PA, given the commonplace practice of  
5 oversizing the patch in younger patients to accommodate for later growth, may also result in  
6 abnormal renal blood flow and contribute to the persistence of the hypertensive state.

7

## 8 **METHODS**

9           Aortorenal blood flow was retrospectively studied using patient-specific fluid-structure  
10 interaction (FSI) simulations in a child that was treated for a SAAC. Subsequently, the impact of  
11 the most commonly undertaken surgical repairs (TAB and PA) on aortorenal blood flow was  
12 analyzed. The study was approved by the University of Michigan Board of Review  
13 (HUM00112350 and HUM00006223).

14           ***Patient history.*** A 9-year-old girl was referred to the authors' institution with a diagnosis  
15 of middle aortic syndrome and renin mediated hypertension. Her initial elevated blood pressures  
16 in the 130-150/90-95 mmHg range were only modestly improved to the 140/80 mmHg range  
17 following treatment with a beta-blocker and calcium channel blocker. In addition, she initially  
18 complained of lower extremity weakness and fatigue that was progressive with activity. Duplex  
19 Doppler ultrasonography estimated a pressure gradient of 58 mmHg across the SAAC. She was  
20 considered an appropriate candidate for surgical repair of the abdominal aortic coarctation.

21           ***Imaging data.*** Preoperative anatomy and hemodynamic data were obtained using duplex  
22 Doppler ultrasonography, computed tomography angiography (CTA) and phase contrast magnetic  
23 resonance imaging (PC-MRI). CTA imaging revealed a SAAC of 15 mm in length, with a 2.5 mm

1 anterior-posterior diameter, and no renal artery involvement (Figure 1). The celiac artery (CA) and  
2 superior mesenteric artery (SMA) arose from the coarctation itself, and both exhibited ostial  
3 narrowings. Extensive collaterals circumvented the coarcted aorta, with an intact inferior  
4 mesenteric artery (IMA) being the dominant source of blood flow to the intestines. The internal  
5 mammary arteries were enlarged and communicated with the epigastric arteries that had multiple  
6 collaterals to the lower extremities and abdominal visceral organs. MRI examinations performed  
7 at 10-day and 1-year after the TAB provided postoperative data for analysis.

8 *Thoracoabdominal bypass.* The basis for choosing a TAB over a PA was that the 2.5 mm  
9 diameter of the coarctation and the involvement of the CA and SMA would have made an  
10 aortoplasty inordinately challenging and risky. In this case a midline abdominal incision was made  
11 from the xiphoid to the pubis, followed by medial visceral rotation of the left colon, to provide  
12 exposure of the entire abdominal aorta.

13 The supra celiac aorta was occluded with a Satinsky clamp, following which a 14 mm  
14 polytetrafluoroethylene (PTFE) bypass graft was anastomosed to a lateral aortotomy. The  
15 proximal aorta was occluded for 17 minutes during which time blood flow to the lower extremities  
16 and abdominal viscera, although reduced, was maintained through the preexisting large  
17 retroperitoneal and abdominal wall collaterals. The graft was then clamped just beyond its aortic  
18 origin and antegrade aortic blood flow was restored following removal of the supraceliac aortic  
19 clamp. The graft was passed behind the left kidney and then anastomosed in an end-to-side manner  
20 to a lateral aortotomy just above the IMA (Figure 1). During the distal anastomosis, the infrarenal  
21 aorta was occluded for a time similar to that of the proximal anastomosis.

22 ~~*Thoracoabdominal bypass.* The basis for choosing a TAB over a PA was that the small~~  
23 ~~diameter of the coarctation and the involvement of the CA and SMA would have made an~~



~~aortoplasty inordinately challenging and risky. A 14 mm polytetrafluoroethylene (PTFE) bypass graft originating from the supra-celiac aorta was carried to the infra-renal aorta proximal to the IMA (Figure 1). The procedure was performed without complications and the patient was discharged with resolution of her lower extremity discomfort. However, she remained mildly hypertensive postoperative and at 1 year follow up; she remained on a low dose calcium channel blocker with resting blood pressures in the 110-115/65-70 mmHg range.~~

~~**Kidney Size.** Analyzing the preoperative and 10 day follow up imaging data, an increase in kidney length was observed. Following this finding, p~~Preoperative and 10-day postoperative kidney volumes were measured using semi-automatic segmentation tools in Mimics version 21.0 (Materialise NV, Leuven, Belgium).

~~**Computational modeling.** Patient-specific FSI simulations<sup>9</sup> were performed to assess preoperative blood flow and compare the hemodynamic performance of TAB versus PA using a “virtual testing” paradigm (Figure 2).<sup>10</sup> First, a preoperative model was created and calibrated to match the anatomical and hemodynamic clinical data (Figure 23). Then, the calibrated preoperative model was adapted to reflect six surgical interventions (Figure 34), including three different TABs with 12 mm, 14 mm and 16 mm diameters, respectively (TAB-12mm, TAB-14mm and TAB-16mm); and three different PAs producing increases in aortic diameters of 0%, 30% and 50% (PA-0%, PA-30% and PA-50%) relative to the native aorta. Additionally, a control case was constructed by adjusting the preoperative model to produce a healthy anatomy without coarctation and collateral vessels (Appendix Figure 3).~~

~~The preoperative and six surgical repair All models were constructed from the CTA image data using the cardiovascular-CRIMSON (CardiovasculaR Integrated modeling-Modeling and simulation-SimulatiON) software-version 2017.07.01, developed by King’s College London~~

1 (London, UK) and the University of Michigan (Ann Arbor, MI) under the support of the European  
2 Research Council CRIMSON.<sup>11</sup> Besides the vascular anatomy, each FSI model requires  
3 specification of arterial wall material properties (thickness and stiffness) as well as outflow  
4 boundary conditions at each branch. These boundary conditions represent the compliance and  
5 resistance of the distal vasculature not included in the anatomical model. The wall properties and  
6 outflow boundary conditions were calibrated to match the simulation results with the clinically  
7 acquired flow and pressure data and achieve reasonable physiologic regional flow distributions<sup>13</sup>  
8 (Figure 23).<sup>12</sup> The methods for specification of the boundary conditions and material properties  
9 are reported in detail in the Appendix. In the control case, the boundary conditions were tuned to  
10 match the preoperative flow splits and a blood pressure appropriate for this patient's size and age  
11 (96/65 mmHg).<sup>13</sup> In the postoperative models, cardiac output and outflow boundary conditions  
12 were kept the same as preoperative; with the exception of the supra-aortic arteries, where the  
13 outflow boundary conditions were adjusted to reproduce literature data on regional flow  
14 splits.<sup>14</sup> ~~maintain similar flow rates as preoperative. By doing so, the effects of cerebral~~  
15 ~~autoregulation were taken into account.~~

16 **Computations.** -Blood was modeled as an incompressible Newtonian fluid with a density  
17 of 1,060 kg/m<sup>3</sup> and a dynamic viscosity of 4.0 Pa·s. Computations were performed using the  
18 CRIMSON Navier-Stokes flow solver on 160 cores at the University of Michigan high-  
19 performance computing cluster ConFlux. Simulations were run until cycle-to-cycle periodicity  
20 was achieved in the pressure fields, this typically took three to five cycles. Computation time per  
21 cardiac cycle was approximately 48 hours.

22

23

## 1 RESULTS

2 Postoperative course. Complete resolution of the patient's lower extremity discomfort was  
3 evident in the early postoperative period. Her serum creatinine which ranged from 0.48 to 0.57  
4 mg/dL preoperatively, decreased to 0.28 to 0.3 mg/dL postoperatively. However, she remained  
5 mildly hypertensive during her postoperative hospitalization, and at 1-year follow-up she remained  
6 on a low dose calcium channel blocker with resting blood pressures in the 110-115/65-70 mmHg  
7 range.

8 *Preoperative Simulation.* The baseline preoperative model successfully reproduced the  
9 patient's hemodynamic data, as documented in a comparison between clinical data and simulation  
10 results at different locations in the circulation (Figure 23). The computed flows were all within 5%  
11 of the clinically measured data, and computed pressures were within 10%.

12 The FSI simulation results revealed a pressure gradient of 55 mmHg across the coarctation  
13 at peak-systole (Figure 45), which matched the pressure gradient derived from duplex Doppler  
14 ultrasonography (58 mmHg). Additionally, disturbed flow patterns were present distal to the  
15 coarctation which propagated into the renal arteries. Assessment of the renal artery flow and  
16 pressure waveforms revealed diastolic dominated renal flows with high frequency oscillations  
17 (Figure 45 and Video 1). Renal artery pressure was markedly lower than ascending aortic pressure.

18 In the control case, systolic dominated renal flows without high-frequency disturbances  
19 were found. The results for the control anatomy are presented in Video 1 and Appendix Figure 3.  
20 A direct comparison of the pressure and flow waveforms between preoperative and control cases  
21 is reported in Figure 5.

22

1            **Postoperative Simulations.** The computed mean flows at the outlets of the preoperative  
2 model and all six surgical repair models (Table 1) were revealing. All six interventions successfully  
3 reduced pressures at the ascending aorta (Figure 6) and increased renal artery flow rates (Table 1).  
4 Furthermore, all surgical repairs resulted in systolic dominated flow waveforms (Figure 7), with a  
5 reduction of the high frequency flow and pressure disturbances in the renal arteries (Figures 7 and  
6 8). Although most postoperative simulations retained some degree of the high frequency  
7 oscillations, the PA-0% eliminated the high frequency oscillations completely.

8            The flow waveforms from the TAB-14mm simulation were compared with the PC-MRI  
9 data at 1-year follow-up (Figure 9). The patient's cardiac output decreased during follow-up (-  
10 13%, from 3.9 to 3.2 L/min). The shape of the waveform changed as a result of a reduction in  
11 ventricular afterload following surgery. The computed (TAB-14mm) and 1-year follow-up PC-  
12 MRI data on flow through the bypass documented an excellent match: the percentages of cardiac  
13 output through the bypass were 38% and 39% for the computations and the PC-MRI data,  
14 respectively.

15            **Kidney Size.** Considerable changes in the kidney ~~length volumes~~ were noted at 10-day  
16 follow-up. To accurately quantify the change in kidney size, volumetric measurements of both  
17 kidneys were obtained (Figure 109). Right and left kidney lengths increased from 3.4 to 3.85 cm  
18 (+13%) and from 3.8 to 4.6 cm (+21%), respectively. Right and left kidney volumes increased  
19 from 50.3 to 79.6 cm<sup>3</sup> (+58%) and 51.5 to 92.0 cm<sup>3</sup> (+79%), respectively. The observed increments  
20 in kidney volume reflected the calculated increases in right and left renal flow from the TAB-  
21 14mm FSI analysis (+9% and +26%, respectively).

22

23

## 1 **DISCUSSION**

2 Abdominal aortic coarctation is a rare vascular disease recognized most frequently in  
3 pediatric-age patients. The aortic narrowings are commonly associated with ostial stenoses of the  
4 celiac, superior mesenteric, and renal arteries.<sup>15</sup> This is clinically referred to as the middle aortic  
5 syndrome, which manifests in most patients with drug therapy resistant arterial hypertension.<sup>16</sup>

6 Classic canine experiments noted that the location of the abdominal coarctation plays a key  
7 role in the presence of hypertension.<sup>17</sup> Hypertension is commonly observed in cases where the  
8 coarctation is suprarenal or involves the renal arteries. Conversely, hypertension is mostly absent  
9 when the coarctation is distal to the renal arteries. An investigation by Scott et al.<sup>18</sup> of canine  
10 hypertension due surgically induced coarctation of the aorta that resulted in hypertension at 5 to 7  
11 weeks, noted that transposition of a kidney to a level above the coarctation and contralateral  
12 nephrectomy resulted in disappearance of hypertension. These earlier experiments suggest that  
13 disturbed aortorenal blood flow contributes to hypertension in abdominal coarctation.

14 When treating middle aortic syndrome, conventional surgical reconstructive procedures  
15 and catheter-based interventions are favored over long-term drug therapy.<sup>1,7,19-22</sup> Operative  
16 planning is usually derived solely from preoperative imaging.<sup>23</sup> Surgical decisions are often based  
17 on technical issues at hand, rather than aiming to restore normal aortorenal blood flow.  
18 Unfortunately, endovascular balloon dilation with or without stenting of abdominal aortic  
19 narrowings has had limited use with mixed early results and few long-term successes. Open  
20 operations, such as TAB and PA, have been the most common form of treating abdominal aortic  
21 coarctations. These operations often lead to improved hypertension control, yet most cases still  
22 depend on antihypertensive therapy to maintain normal blood pressures for gender and age.

1           Many factors go into decision making for performing a PA versus a TAB. A PA is favored  
2 in most instances of a limited aortic coarctation distant from the CA, SMA and renal arteries. When  
3 assessing the long-term benefits of PA in younger patients, the patch is intentionally oversized to  
4 account for the child's expected growth. Nevertheless, the appropriate degree of patch oversizing  
5 has not been established. Likewise, the effects on renal artery blood flow accompanying a  
6 disproportionately enlarged aorta following a PA are unknown.

7           A TAB is the procedure of choice when treating more severe coarctations with abdominal  
8 aortic diameters of only a few millimeters. In this case, a PA would have near-overlapping sutures  
9 from the lateral walls of the patch. In the past, the authors have recommended a wide range of  
10 TAB diameters related to age, with the intent that the bypass diameter would at least be 60% to  
11 70% of the predicted adult aorta.<sup>1</sup> These recommendations may be logical, but as noted with PA  
12 oversizing, the science behind such is meager.

13           ***Clinical Experience.*** Recently, the authors reviewed their experience with 155 children  
14 having renal artery stenotic disease and renovascular hypertension.<sup>6</sup> Hypertension outcomes were  
15 better in children treated with renal artery reconstructions alone compared to those requiring  
16 additional aortic procedures. The hypertension cure, improved, and failure rates in patients without  
17 aortic pathology (n=98) were 50%, 34% and 16%, respectively. These outcome rates were 33%,  
18 59% and 8% in patients additionally treated with PA (n=28); and 35%, 50% and 15% in patients  
19 additionally treated with TAB (n=29). Given the poorer outcomes in patients undergoing  
20 concomitant aortic procedures, one must question whether abnormal aortorenal flow remains after  
21 surgery, and if differences exist between surgical repair with TAB and PA.

22           ***Computational Modeling.*** Computational modeling is a widely used method in  
23 engineering fields that can be applied to study complex flow dynamics. Image-based

1 computational tools have been developed for cardiovascular disease research,<sup>24,25</sup> medical device  
2 evaluation<sup>22</sup> and, more recently, virtual planning of surgical interventions.<sup>9</sup> While in other  
3 engineering fields the ‘virtual testing’ paradigm has largely replaced the traditional ‘build-and-  
4 test’ (e.g. trial and error) paradigm, this is not yet the case in the medical field. As evident in the  
5 current investigation, the value of computational modeling is apparent in preoperative  
6 determination of the therapeutic impact of different sizes of TAB and PA in patients with the  
7 midaortic syndrome.

8         Computational modeling in this investigation provided data of much higher spatial (up to  
9 0.05 mm) and temporal (0.025 ms) resolution than available in any contemporary imaging test.  
10 This high-resolution data revealed an unexpected and potentially relevant finding of high  
11 frequency disturbances in the renal arteries preoperatively that could explain an increased renin  
12 release in the kidneys, resulting in secondary hypertension. Persistent high frequency disturbances  
13 were also found in the postoperative models and might explain the continuing hypertension  
14 following both TAB and PA interventions in patients undergoing concomitant renal artery  
15 reconstructions.

16         Besides characterization of preoperative aortorenal blood flow, this study also analyzed the  
17 impact of different TAB diameters and degree of PA oversizing. In total, six different surgical  
18 treatment options were studied: three TAB diameters and three levels of PA oversizing. All  
19 surgical interventions resulted in reduced aortic pressures, and increased renal flows with  
20 restoration of systolic-dominated waveforms.

21         An unexpected finding of this investigation was that most surgical repairs resulted in a  
22 reduction in renal artery pressures (Figure 8). This acute response of the system, which does not

1 account for any auto-regulatory processes following the surgery, is reflective of the large  
2 reductions in aortic pressures in all postoperative models (Figure 6).

3         Importantly, various degrees of high frequency disturbances persisted postoperatively, the  
4 exception being the treatment with a 0% PA which eliminated the high frequency disturbances  
5 completely. These results suggest that excessive PA oversizing and TAB lead to high frequency  
6 disturbances that may contribute to continued renin-mediated hypertension.

7         In the TAB operations, the high frequency disturbances could be explained by the turbulent  
8 mixing of antegrade flow through the remaining aortic stenosis and retrograde flow through the  
9 TAB. Changing the TAB graft diameter did not significantly impact the persistence of high  
10 frequency disturbances. Such flow abnormalities could explain why the patient in the present case  
11 report, who had undergone a TAB repair, was still dependent on anti-hypertensive medication at  
12 1-year follow-up. In an oversized PA, the dilated segment of the reconstruction induces flow  
13 disturbances. Flow clearly shows complex recirculation and vortices in the region of the patch  
14 (Figure 11), similar to what is observed in aneurysmal disease. The absence of dilation in the PA-  
15 0% case explains the lack of disturbances in this model. Furthermore, it may also explain the  
16 reduced hypertension cure rates of renal artery revascularizations in the authors' larger series of  
17 patients requiring concomitant aortic procedures.

18         Historically, renin-mediated hypertension has been linked to low perfusion pressure and  
19 low renal blood flow.<sup>23</sup> The high frequency flow oscillations observed in the present work have  
20 not been described in the earlier literature. The most likely explanation for this is that contemporary  
21 clinical measurement devices lack the temporal resolution necessary to detect such high frequency  
22 flow oscillations. It has been recognized that Doppler ultrasonography, CTA and MRI can all be



1 helpful in the evaluation of renovascular disease, but none have, at present, high enough sensitivity  
2 to rule out renovascular disease in a child with a suggestion of that diagnosis.<sup>27</sup>

3  
4 ***Limitations.*** The stiffness properties of the aortic wall could not be calculated with the  
5 available data in this study. Therefore, in the present investigation, the assigned stiffness  
6 parameters were derived from a previous study from our laboratory which characterized aortic  
7 stiffness in a cohort of pediatric patients with aortic coarctation.<sup>28</sup> In that study, the aortic stiffness  
8 was calculated using strain measurements from MRI and invasive pressure measurements from  
9 catheterization.

10 This investigation analyzed aortorenal blood flow in a single patient with a suprarenal  
11 abdominal aortic coarctation. While the results for this patient were clinically-validated,  
12 performing the same analysis in patients with different anatomical features might result in different  
13 outcomes, including the presence of high-frequency disturbances in the renal arteries.  
14 Additionally, the causality between the high frequency disturbances and excessive renin release  
15 should be further investigated. Furthermore, we tested six different surgical interventions with  
16 arbitrary TAB and PA sizes. Performing a parametric study of other patch and bypass sizes and  
17 configurations could result in different outcomes.

18 Furthermore, it is important to note that even though a specific intervention might  
19 theoretically render a better hemodynamic outcome, performance of the procedure itself may be  
20 inordinately challenging and risky, resulting in a technical failure and less successful outcome.  
21 Thus, acceptance of benefits defined by virtual testing must be tempered by clinical judgement  
22 and expertise.

1           Lastly, the results presented here do not take into account any of the vascular auto-  
2 regulations that undoubtedly occur after a vascular reconstruction. The magnitude of the  
3 waveforms, specifically the pressure, might change as a result of systemic vasoreactivity, although  
4 the high frequency disturbances are likely to persist.

5

## 6 **CONCLUSIONS**

7           This study has revealed the presence of high frequency disturbances in renal blood flow  
8 and pressure following operative interventions for SAAC. These previously unrecognized  
9 disturbances may be a fundamental contributor to continued abnormal release of renin, and thus  
10 the basis of the often-seen persistent post-operative hypertension in this patient population.

11           Considerable value resides in computational modeling of vascular surgery procedures.  
12 Patient-specific modeling provides high-resolution hemodynamic information for differing  
13 interventions, and allows preoperative planning for complex procedures, such as those  
14 accompanying aortic reconstructions in young patients with SAAC. Collaborative efforts between  
15 biomedical engineers and clinicians will be essential to providing accurate modeling and  
16 simulation of feasible surgical procedures in this setting.

17

18

19

20

21

22

23

**1 REFERENCES**

- 2 1. Stanley JC, Criado E, Eliason JL, Upchurch GR, Berguer R, Rectenwald JE. Abdominal  
3 aortic coarctation: Surgical treatment of 53 patients with a thoracoabdominal bypass,  
4 patch aortoplasty, or interposition aorto-aortic graft. *J Vasc Surg.* 2008 Nov;48(5):1073–  
5 82.
- 6 2. Fry WJ, Ernst CB, Stanley JC, Brink B. Renovascular hypertension in the pediatric  
7 patient. *Arch Surg.* 1973 Nov;107(5):692–8.
- 8 3. Stanley JC, Fry WJ. Pediatric renal artery occlusive disease and renovascular  
9 hypertension. Etiology, diagnosis, and operative treatment. *Arch Surg.* 1981  
10 May;116(5):669–76.
- 11 4. Stanley JC, Zelenock GB, Messina LM, Wakefield TW. Pediatric renovascular  
12 hypertension: a thirty-year experience of operative treatment. *J Vasc Surg.* 1995  
13 Feb;21(2):212-26; discussion 226-7.
- 14 5. Stanley JC, Criado E, Upchurch GR, Brophy PD, Cho KJ, Rectenwald JE. Pediatric  
15 renovascular hypertension: 132 primary and 30 secondary operations in 97 children. *J*  
16 *Vasc Surg.* 2006 Dec 1;44(6):1219–28.
- 17 6. Coleman DM, Eliason JL, Jackson T, Kershaw DB, Williams DM, Ganesh SK, et al. SS26  
18 Surgical Management of Pediatric Renovascular Hypertension. *J Vasc Surg.* 2017 Jun  
19 1;65(6):138S.
- 20 7. Rumman RK, Nickel C, Matsuda-Abedini M, Lorenzo AJ, Langlois V, Radhakrishnan S,  
21 et al. Disease beyond the arch: A systematic review of middle aortic syndrome in  
22 childhood. *Am J Hypertens.* 2015 Jul 1;28(7):833–46.
- 23 8. Rocchini AP, Rosenthal A, Barger AC, Castaneda AR, Nadas AS. Pathogenesis of

- 1 paradoxical hypertension after coarctation resection. *Circulation*. 1976 Sep;54(3):382–7.
- 2 9. Figueroa CA, Vignon-Clementel IE, Jansen KE, Hughes TJR, Taylor CA. A coupled  
3 momentum method for modeling blood flow in three-dimensional deformable arteries.  
4 *Comput Methods Appl Mech Eng*. 2006;195(41–43):5685–706.
- 5 10. van Bakel TMJ, Lau KD, Hirsch-Romano J, Trimarchi S, Dorfman AL, Figueroa CA.  
6 Patient-Specific Modeling of Hemodynamics: Supporting Surgical Planning in a Fontan  
7 Circulation Correction. *J Cardiovasc Transl Res*. 2018 Apr 8;11(2):145–55.
- 8 11. CRIMSON. The software for Cardiovascular Modelling and Simulation [Internet].  
9 Available from: [www.crimson.software](http://www.crimson.software)
- 10 12. Xiao N, Alastruey J, Figueroa CA. A systematic comparison between 1-D and 3-D  
11 hemodynamics in compliant arterial models. *Int j numer method biomed eng*.  
12 2013;30(2):204–31.
- 13 13. National High Blood Pressure Education Program Working Group on High Blood  
14 Pressure in Children and Adolescents. The fourth report on the diagnosis, evaluation, and  
15 treatment of high blood pressure in children and adolescents. *Pediatrics*. 2004 Aug;114(2  
16 Suppl 4th Report):555–76.
- 17 14. Lantz BMT, Foerster JM, Link DP, Holcroft JW. Regional distribution of cardiac output:  
18 Normal values in man determined by video dilution technique. *Am J Roentgenol*.  
19 1981;137(5):903–7.
- 20 15. Cohen JR, Birnbaum E. Coarctation of the abdominal aorta. *J Vasc Surg*. 1988  
21 Aug;8(2):160–4.
- 22 16. Panayiotopoulos YP, Tyrrell MR, Koffman G, Reidy JF, Haycock GB, Taylor PR. Mid-  
23 aortic syndrome presenting in childhood. *Br J Surg*. 1996;83(2):235–40.

- 1 17. Goldblatt H, Kahn JR, Hanzal RF. STUDIES ON EXPERIMENTAL HYPERTENSION :  
2 IX. THE EFFECT ON BLOOD PRESSURE OF CONSTRICTION OF THE  
3 ABDOMINAL AORTA ABOVE AND BELOW THE SITE OF ORIGIN OF BOTH  
4 MAIN RENAL ARTERIES. *J Exp Med.* 1939 Apr;69(5):649–74.
- 5 18. Scott HW, Bahnson HT. Evidence for a renal factor in the hypertension of experimental  
6 coarctation of the aorta. *Surgery.* 1951 Jul 1;30(1):206–17.
- 7 19. Porras D, Stein DR, Ferguson MA, Chaudry G, Alomari A, Vakili K, et al. Midaortic  
8 syndrome: 30 years of experience with medical, endovascular and surgical management.  
9 *Pediatr Nephrol.* 2013 Oct 18;28(10):2023–33.
- 10 20. Sandmann W, Dueppers P, Pourhassan S, Voiculescu A, Klee D, Balzer KM. Early and  
11 Long-term Results after Reconstructive Surgery in 42 Children and Two Young Adults  
12 with Renovascular Hypertension due to Fibromuscular Dysplasia and Middle Aortic  
13 Syndrome. *Eur J Vasc Endovasc Surg.* 2014 May;47(5):509–16.
- 14 21. Sethna CB, Kaplan BS, Cahill AM, Velazquez OC, Meyers KEC. Idiopathic mid-aortic  
15 syndrome in children. *Pediatr Nephrol.* 2008 Jul 5;23(7):1135–42.
- 16 22. Tummolo A, Marks SD, Stadermann M, Roebuck DJ, McLaren CA, Hamilton G, et al.  
17 Mid-aortic syndrome: long-term outcome of 36 children. *Pediatr Nephrol.* 2009 Nov  
18 15;24(11):2225–32.
- 19 23. Castelli PK, Dillman JR, Smith EA, Vellody R, Cho K, Stanley JC. Imaging of Renin-  
20 Mediated Hypertension in Children. *Am J Roentgenol.* 2013 Jun 23;200(6):W661–72.
- 21 24. Taylor CA, Figueroa CA. Patient-specific modeling of cardiovascular mechanics. *Annu*  
22 *Rev Biomed Eng.* 2009;11:109–34.
- 23 25. van Bakel TM, Arthurs CJ, Nauta FJ, Eagle KA, van Herwaarden JA, Moll FL, et al.

- 1 Cardiac remodelling following thoracic endovascular aortic repair for descending aortic  
2 aneurysms †. *Eur J Cardio-Thoracic Surg.* 2018;0:1–10.
- 3 26. van Bakel TM, Arthurs CJ, van Herwaarden JA, Moll FL, Eagle KA, Patel HJ, et al. A  
4 computational analysis of different endograft designs for Zone 0 aortic arch repair†. *Eur J*  
5 *Cardio-Thoracic Surg.* 2018 Aug 1;54(2):389–96.
- 6 27. Tullus K, Roebuck DJ, McLaren CA, Marks SD. Imaging in the evaluation of  
7 renovascular disease. *Pediatr Nephrol.* 2010 Jun 24;25(6):1049–56.
- 8 28. Sotelo JA, Valverde I, Beerbaum PB, Greil GF, Schaeffter T, Razavi R, et al. Pressure  
9 gradient prediction in aortic coarctation using a computational-fluid-dynamics model:  
10 validation against invasive pressure catheterization at rest and pharmacological stress. *J*  
11 *Cardiovasc Magn Reson.* 2015;17(Suppl 1):Q78.
- 12