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The Influence of Recording Equipment on the Accuracy of Respiratory Rate Estimation from the Electrocardiogram or Pulse Oximeter

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Patient monitors filter electrocardiogram (ECG) and pulse oximeter (PPG) signals prior to output. Would respiratory rate (RR) estimates derived from these signals be more accurate if unfiltered signals were used?

**Methods**

Signal Acquisition: 42 young (18-40 years), and 16 elderly (≥ 70) healthy volunteers took part. Minimally filtered PPG and ECG signals were acquired using laboratory equipment. Filtered signals were acquired from a tethered monitor. Filtered PPG was also acquired from a wireless monitor. Reference RR was obtained from oronasal airflow and chest impedance signals.

RR Estimation: Breaths were detected from the respiratory modulations (Fig. 2) in the time-domain using 3-point peak detection. In the frequency-domain, the RR was identified as the frequency with the maximum FFT power within 6-40 bpm.

Statistical Analysis: The null hypothesis, that the difference between RMSEs obtained using laboratory and routine equipment is zero, was tested using the paired, two-sample t-test at 5\% significance level.

**Results**

The null hypothesis, that filtering had no impact on accuracy of RR estimates was accepted, when using all but two of the estimation methods (Table 1). In one of these instances the filtered signals provided more accurate estimates (blue), and in the other the unfiltered signals gave higher accuracy (red).

**Conclusions**

The accuracy of RRs estimated from PPG and ECG signals differed minimally between minimally filtered and routinely filtered signals in this healthy cohort. We found no evidence to suggest that more accurate RR estimates could be obtained from unfiltered signals in this cohort.

**Future Work**

This is part of a larger study to assess the influence of physiological and technical factors on the accuracy of algorithms for RR estimation from the ECG and PPG.

**Table 1:** The median (quartiles) subject-specific RMSEs of RR estimates derived from ECG and PPG signals. RR was estimated in the time and frequency domains from the three respiratory modulations: AM, FM and BW (as shown in Fig. 2).

<table>
<thead>
<tr>
<th>Signal</th>
<th>Time-domain Methods</th>
<th>Frequency-domain Methods</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>AM</td>
<td>FM</td>
</tr>
<tr>
<td>PPG</td>
<td>Minimally filtered</td>
<td>3.4(2.9 - 4.6)</td>
</tr>
<tr>
<td></td>
<td>Tethered Monitor</td>
<td>4.0(2.6 - 5.0)</td>
</tr>
<tr>
<td></td>
<td>Wireless Monitor</td>
<td>3.9(3.0 - 4.7)</td>
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<tr>
<td>ECG</td>
<td>Minimally filtered</td>
<td>3.7(2.6 - 4.5)</td>
</tr>
<tr>
<td></td>
<td>Tethered Monitor</td>
<td>3.0(2.3 - 4.7)</td>
</tr>
</tbody>
</table>

**References**


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